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### INTRODUCTION

- Acute entrapment of the facial nerve in the narrow confines of the temporal bone secondary to viral inflammation may result in high grade neural injury and subsequent aberrant neural regeneration
- Such injury occurs in 15-30% patients, Bell's palsy resulting in irreversible postparalysis facial palsy (Fig. 1)
- Clinical data varies regarding efficacy of decompression surgery on facial outcome
- facial nerve entrapment and has been described



No animal model examining Figure 1. Post-paralysis right facial palsy. A: Involuntary eye closure with pucker. B: Neck contraction Impaired oral subsequent decompression commissure excursion and involuntary eye closure with smile.

## DEVICE DESIGN AND MANUFACTURE

- A fully implantable device to induce compression around rat facial nerve was designed for wireless, long-term implantation (Fig. 2)
- Wirelessly relays pressure data hourly to external receiver
- Receiver logs data into SD card or directly to computer, can record multiple device inputs simultaneously.
- components integrated onto a single printed circuit board (PCB), coated in medical-grade silicone, and gas sterilized (EtO)
- Combined with existing rat model for evaluating facial nerve function based on whisker movements





board with (4)

# **Quantitative Model for Decompression Surgery in Bell's Palsy** R. Malka<sup>1,2</sup>, D. Guarin<sup>2</sup>, S. Mohan<sup>2</sup>, P. Gorelik<sup>3</sup>, C. Knox<sup>2</sup>, O. Mazor<sup>3</sup>, T. Hadlock<sup>2</sup>, N. Jowett<sup>2</sup>

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## IN VIVO VALIDATION

Figure 2. (a) Implant deconstructed without silicone encasement, showing (1) subcutaneous injection port, (2) hydraulic cuff, (3) printed circuit microcontroller (Simblee), (5) magnetic switch, and (6) pressure sensor. (b) Implant with parts assembled and encased in silicone. Final weight 10-15g.

- functional impairment from device placement
- count or thickness in nerve proximal, within, or distal to cuff
- showed complete neurotmesis and pervasive regeneration



Figure 3. Left: Comparison of compressive pressure (blue) and facial nerve function (orange) over varying applied compressive forces. Low pressure (0-100mmHg) compression did not result in facial nerve functional impairment, while high-pressure (> 300mmHg) showed immediate loss of facial nerve function with significant remaining impairment after 6 weeks of recovery. Gradual, > 50% reduction in facial nerve function was seen at ~250mmHg compression, with full recovery after decompression. Right: Confocal fluorescence imaging of rat facial nerves exposed to low, medium, and high-pressures from implanted pressure cuff. Facial nerve axons exposed to low-pressures showed relatively unchanged axon caliber along the length of the nerve. Mediumpressure application revealed increased axon caliber variability with greater number of regenerating, small caliber axons. With high-pressure, near-complete axonal regeneration is suggested as the vast majority of stained axons are small, regenerating fibers.

Three animals implanted and pressures maintained in low (0-100mmHg), medium (200-300mmHg), and high (300-500mmHg) ranges for 5 days before decompression, followed for 10 weeks post-decompression or until full recovery observed. Animals sacrificed for nerve staining at 10 weeks.

No pressurization during first 3 days post-implantation, demonstrated no

Low-pressure animal maintained full function of nerve, no change in axon

Medium-pressure animal showed gradual loss of > 50% function within 1 day of pressure exceeding 250mmHg, with full functional recovery after decompression. Histology suggested partial axonotmesis and regeneration

High-pressure animal immediately lost function throughout compressive period and only recovered to ~50% function after 10 weeks. Histology

## Pressure accuracy and

- precision within desired range (Fig. 4)
- Device lifespan of more than 9 12mm coin cell battery
- Cuff pressure induced maintained and hypertonic injection in subcu port

- surgery



with implant visible on back.







## DEVICE VALIDATION EX VIVO

weeks with with



Figure 4. (a) Dynamic pressure monitoring shows return to within two seconds of rapid pressurization. (b-c) **solution** Static pressure monitoring held over multiple days (b) shows error less than 20mmHg from analog pressure values (c).

## DEVICE IMPLANTATION AND REMOVAL

Surgical implantation described in Figure 4. Implant tolerated > 3 weeks without extrusion, inflammation, strong foreign body response, autotomy, or device failure

Device removed at desired timepoint to simulate decompression

Figure 5. (a) The cuff and device in place before suturing closed, showing device sitting in pocket above scapulae and cuff tunneled through to whisker pad incision. (b) Placement of the cuff around the marginal and buccal branches of the facial nerve. (c) Animal 3 days post-operatively

### CONCLUSIONS

A low-cost implantable device to apply and monitor extrinsic pressure on a nerve trunk to model entrapment neuropathy has been described

Quantitative measure of neural compartment pressure in vivo may be compared against function in real-time using the rat facial nerve model

Model able to recapitulate Bell's-like phenomenon in rats, showing both full recovery and poor recovery outcomes